



Nanostructured Lipid Carriers: The Perfectness of Imperfectness

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Short Communication

Nanostructured Lipid Carriers (NLC), developed at the turn of millennium [1] are lipid-based nanoparticles composed of binary mixture of solid lipid and liquid lipid [2]. To obtain the blends for the particles matrix, solid lipids (fats) are mixed with liquid lipids (oils), preferably in the ratio of 70:30 up to a ratio of 99.9:0.1 [3]. This colloidal delivery system is stabilized in an aqueous surfactant solution. They exhibit mean particle size in the submicron range, ranging from approximately 40 nm to 1000 nm [4,5]. The basis of an NLC formulation is to produce particles in which the oil is incorporated into the core of the solid lipid and the drug is solubilized in the oily core. The resulting matrix of lipid particles shows imperfections in the crystal lattice (low crystallinity index [6]), and leaves enough space to accommodate drug molecules (higher encapsulation efficiency [7]), thus leading to improved drug payload [8,9]. The amorphous solid structure results in enhanced physical stability [10]. Moreover, by modulating the amounts of oils added to the formulation, the matrix remains solid at room temperature and body temperature, and as such controlled drug release can be realized [11-14].

The usual methods for preparation of NLC include microemulsion method, solvent evaporation method, solvent diffusion method, emulsion-evaporation and low temperature-solidification technique, film dispersion-ultrasonic method and High Pressure Homogenization (HPH) [15]. Owing to its prominent merits of possibility of large scale production and opportunity to sterilize the preparation, HPH technique is by-and-large utilized. However, the demerits of hot homogeneous technique are that: a) the high heating temperature promotes degradation of heat-labile active compounds, b) instability of NLC induced by reduced emulsifying capacity of low cloud surfactants as a result of their exposure to high temperatures, and c) in the course of homogenization, the hydrophobic drug partially migrates to the aqueous phase resulting in low entrapment efficiency [16]; on the other hand at hot state, lipophilic compound solubility is increased in aqueous phase and thereupon the crystallization of it during cooling, since solid matrix of lipid does not allow return of the bioactive within itself [17].

NLC are promising nanocarriers for lipophilic molecules [18]. This may be due to their potential to increase the solubility of lipophilic drugs [19]. More importantly, since the internalization of lipid nanoparticles into cancerous cells is faster, it has greater potential in cancer therapy [20,21]. These solid lipid nanoparticles of the second generation, which are often used for delivery systems of lipophilic actives offer many benefits. They include: a) low toxicity [22], b) their particulate matrix is easily biodegraded resulting in non-toxic degradation products [23], c) the ability to incorporate lipophilic and hydrophilic drugs [24], d) its ability for drug targeting [25], e) the ability to immobilize the drug in the solid particle matrix yielding in protection of the incorporated drug from degradation [26], f) easy production process and feasibility for large scale production [27], g) provides an opportunity to avoid the use of organic solvents [28] and (h) cheap excipients e.g. lipids and stabilizers.

In recent years, NLC have been intensively investigated for administration of drugs by various pharmaceutical application routes, i.e. peroral [29], dermal [30], parenteral [31], pulmonary [32,33] and ocular [34,35]. However, frequently most studies have been focused on topical application of NLC perhaps for their unique positive features. These features are: a) film formation and subsequent adhesion of nanosized particles to the skin surface which provides an occlusion effect with a reduction in the transdermal water loss [36-38]. It has been postulated that the resulting hydration of the skin's outermost layer (stratum corneum) is attributed to a reduction in corneocyte packing and a widening of the inner-corneocyte gaps, hence facilitating drug penetration into the deeper skin strata [39-41], b) skin mucosa penetration is feasible due to nanosize [42,43] and c) enhanced

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skin bioavailability and chemical stability of the bioadditives as well as physical stability of the lipid nanoparticles as topical formulations [38].

Pulmonary drug delivery route represents a potential route for the local treatment of airway diseases and systemic administration of poorly water-soluble drugs that indicate low bioavailability *via* other administration routes i.e. oral and dermal routes [44-46]. Systemic disorders may be cancer, diabetes and immune deficiencies [5]. This route is most favourable due to benefits such as: a) non-invasive, b) lack of first-pass hepatic metabolism and the lungs are well perfused, with blood flow in the vicinity of 5 L/min which helps in drug absorption and distribution [47], c) large surface area (alveoli; $\approx 100 \text{ m}^2$) for absorption, d) relatively slow degradation due to low enzyme activity [48,49]. However, there are hurdles associated with this route. These include: a) inhalation of certain surfactants which may cause lung inflammation [44] and b) fibrosis may occur due to accumulation of surfactant in the lung tissue over prolonged dosing of NLC which may lead to interstitial lung damage and ultimate loss of its elasticity [50]. According to Jaques and Kim, application of NLC to the lower respiratory tract can be realized with particle size below 500 nm, leading to deposition in all lung regions due to an increased diffusional mobility [51].

In view of parenteral application, NLC ability to increase drug load efficiency and prolong exposure of tumour cells to antineoplastic agent, Enhanced Permeability and Retention (EPR) effect may lead to improved drug concentration in the cancerous tissues after systemic administrations (intravenous and intraperitoneal) and subsequently increased therapeutic effect of the antitumour drug [52-54].

In the context of ophthalmic application, traditional ocular drug delivery systems such as eye drops is very poor because eye is protected by a series of complex defensive mechanisms that make it difficult to achieve an effective drug concentration within target area of the eye [55]. The anatomical and physiological constraints include poor corneal permeability, nasolacrimal drainage effect, and short retention time in the precorneal area [56]. With its unique benefits, NLC colloidal carrier system may be better placed to offer improved drug availability either by facilitating transcorneal penetration or by increasing the precorneal residence time.

With these above elaborated facts, surely, one could unequivocally state that “the perfectness” of the NLC resonates with its “imperfectness” in its crystalline structure. With these superb unique features that NLC system harbours, there is no doubt that someday, they may be fully exploited. It is therefore tempting to say that NLC may be heading to be the most successful lipid delivery system after liposomes.

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